

# FEBio: An Open-Source Multiphysics Finite Element Software for Biomechanics and Biophysics

Initiative for Computational Science and Engineering (iCSE) Research Day

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# FEBio Project (febio.org)

- Co-developers

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  - Professor of Biomedical Engineering, University of Utah
- Steve Maas, Ph.D.
  - Software Developer, University of Utah
- Gerard A. Ateshian, Ph.D.
  - Professor of Mechanical Engineering, Columbia University

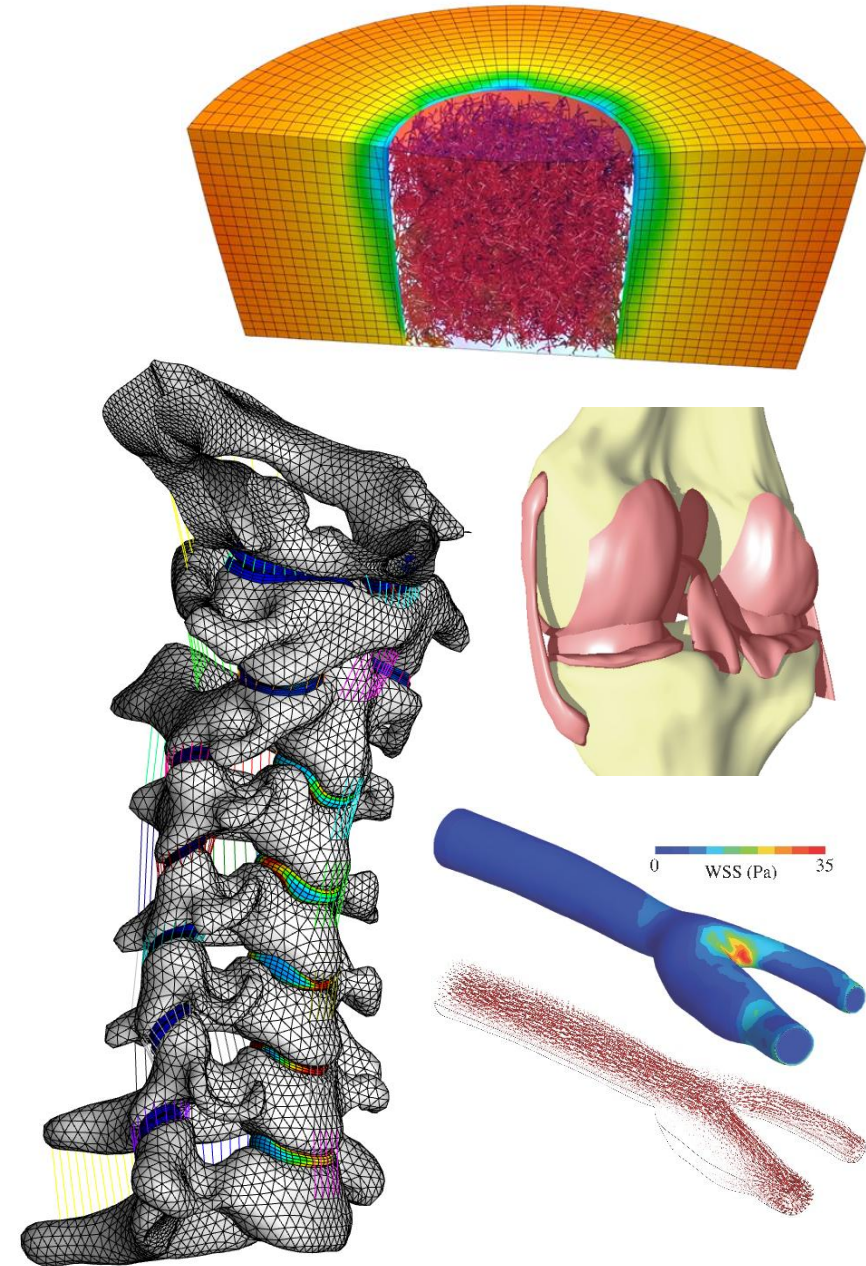


- Pillars of Project

- Target the biomechanics community by focusing on features and simulation capabilities that are relevant to the field
- Freely available, easy to extend
- Thorough documentation; support and outreach to the community

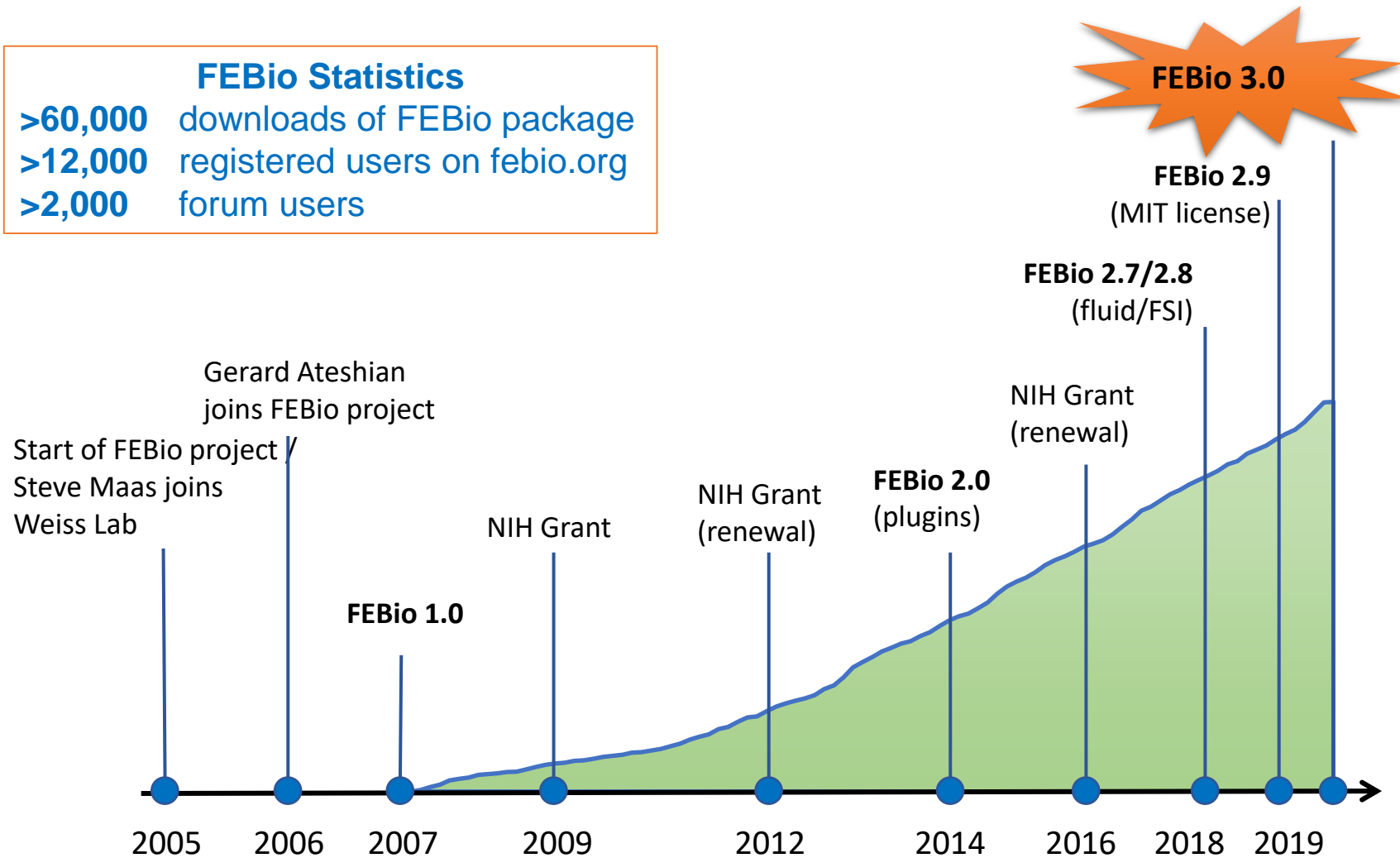
# Overview of Key Features

- Physical scale from cells and subcellular structures to tissues, organs, and whole body.
- Multiphysics - mechanics of solids, fluids and mixtures with growth/remodeling, reaction/diffusion, electrokinetics.
- Constitutive models specific to biomechanics and biophysics – anisotropy, viscoelasticity, multiphase materials, reactions, active contraction, viscous fluids, material evolution.
- Dynamic effects, residual strain, active contraction, interstitial fluid transport, fluid-solid interaction, frictional contact and sliding, interfacial mass transport and electrical conduction.



# Brief History of FEBio

**FEBio Statistics**  
>60,000 downloads of FEBio package  
>12,000 registered users on febio.org  
>2,000 forum users



# Governing Equations

- Equations are based on mixture theory. A mixture consists of any number of constituents  $\alpha$  occupying the same elemental region. The apparent density of constituent  $\alpha$  is denoted by  $\rho^\alpha$ .

- Mass balance

$$\frac{\partial \rho^\alpha}{\partial t} + \operatorname{div}(\rho^\alpha \mathbf{v}^\alpha) = \hat{\rho}^\alpha$$

- Linear momentum balance

$$\rho^\alpha \mathbf{a}^\alpha = \operatorname{div} \boldsymbol{\sigma}^\alpha + \rho^\alpha \mathbf{b}^\alpha + \hat{\mathbf{p}}_d^\alpha$$

- Entropy inequality

$$\sum_\alpha -\boldsymbol{\tau}_d^\alpha : \mathbf{L}^\alpha + \hat{\mathbf{p}}_d^\alpha \cdot \mathbf{u}^\alpha + \hat{\rho}^\alpha \left( \mu^\alpha + \frac{1}{2} \mathbf{u}^\alpha \cdot \mathbf{u}^\alpha \right) \leq 0$$

- Coulomb's law

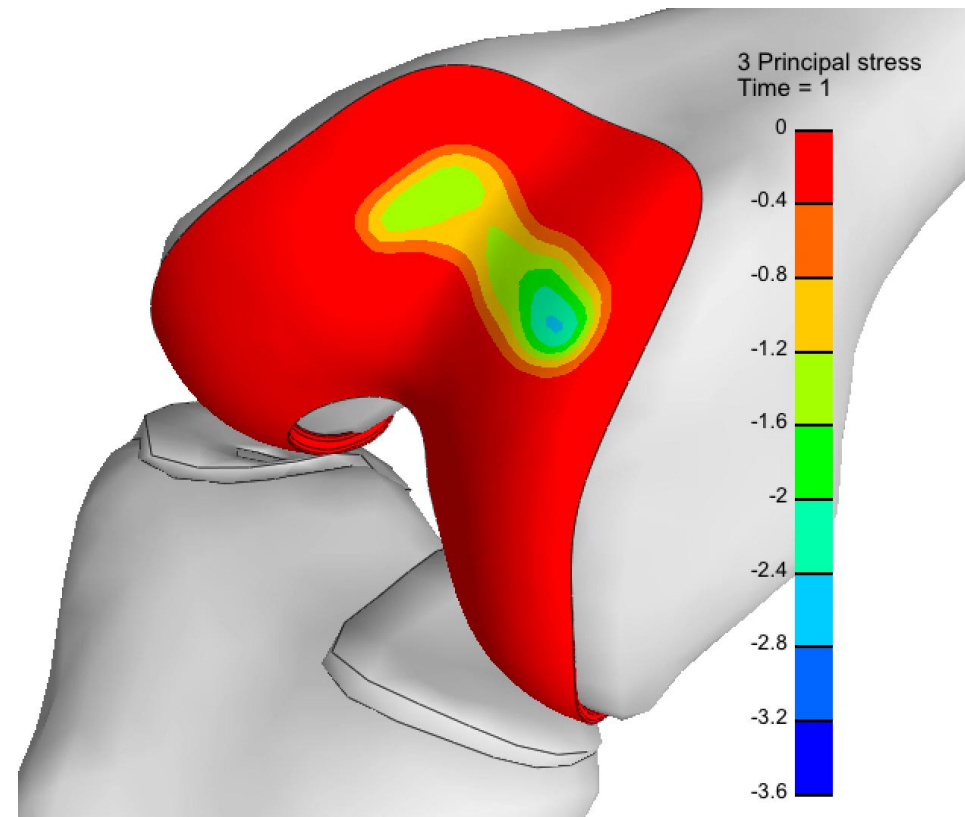
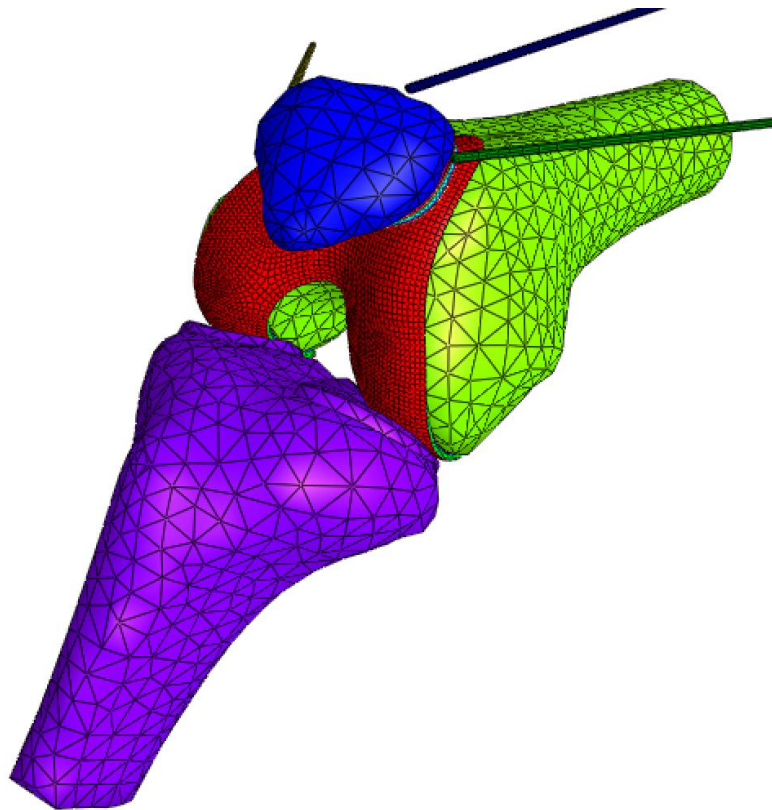
$$\mathbf{b}^\alpha = -\frac{z^\alpha F_c}{M^\alpha} \operatorname{grad} \psi$$

- Electroneutrality

$$\sum_\alpha z^\alpha \frac{\rho^\alpha}{M^\alpha} = 0$$

# Solid-Fluid Mixtures: Biphasic Theory

- First implementation of mixture theory in FEBio (2006)
- Biphasic contact implemented in 2010

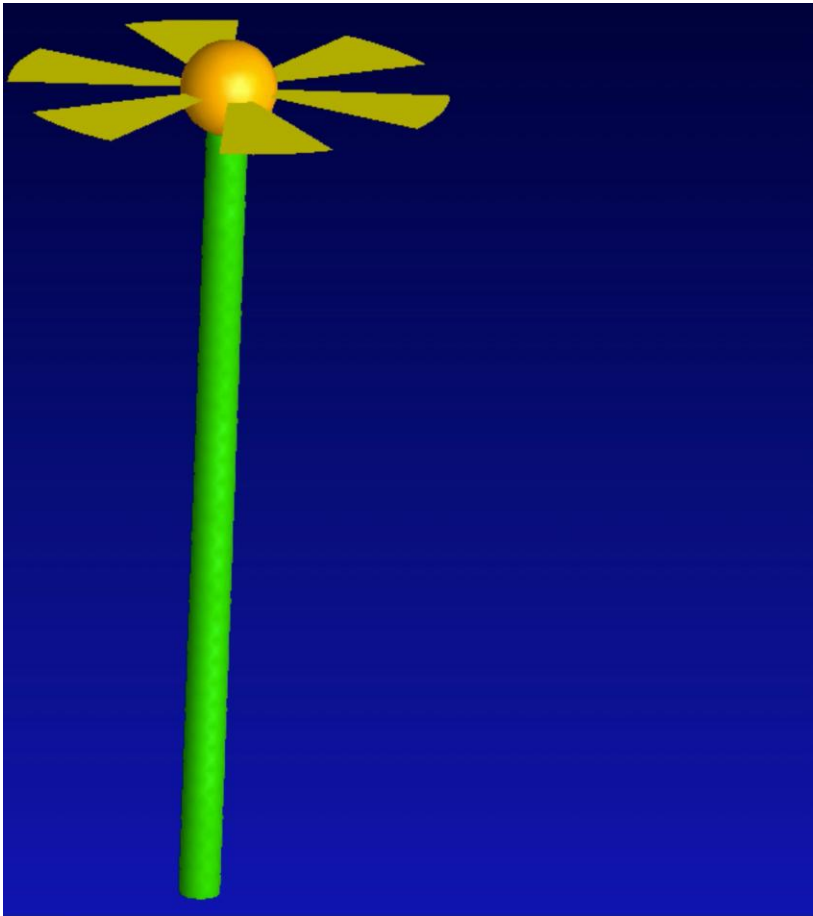


# Mixture of Solid, Solvent and Neutral Solute

- Mauck, Hung, Ateshian (2003)
  - Solute has negligible volume fraction
  - Friction between solute and solvent models classical Fick's law
  - Friction between solute and solid matrix models hindrance
  - Solute may be partially excluded from tissue pore space (steric effect)
  - Account for osmotic pressure
- FEBio implementations
  - Ateshian, Albro, Maas, Weiss (J. Biomech. Eng. 2011)
  - Contact interface: Ateshian, Maas, Weiss (J. Biomech. 2013)
- Solute mass balance
  - $\frac{\partial c^\alpha}{\partial t} + \text{div}(c^\alpha \mathbf{v}^\alpha) = 0$
  - $\frac{1}{J^s} \frac{D^s(J^s \varphi^f \tilde{\kappa} \tilde{c}^\alpha)}{Dt} + \text{div} \mathbf{j}^\alpha = 0$
  - $\mathbf{j}^\alpha = \varphi^f c^\alpha (\mathbf{v}^\alpha - \mathbf{v}^s)$  =solute molar flux relative to solid

# Biphasic-Solute Theory

- Solute osmotic pressure



- Solute pumping

- Due to friction between solute and solid matrix



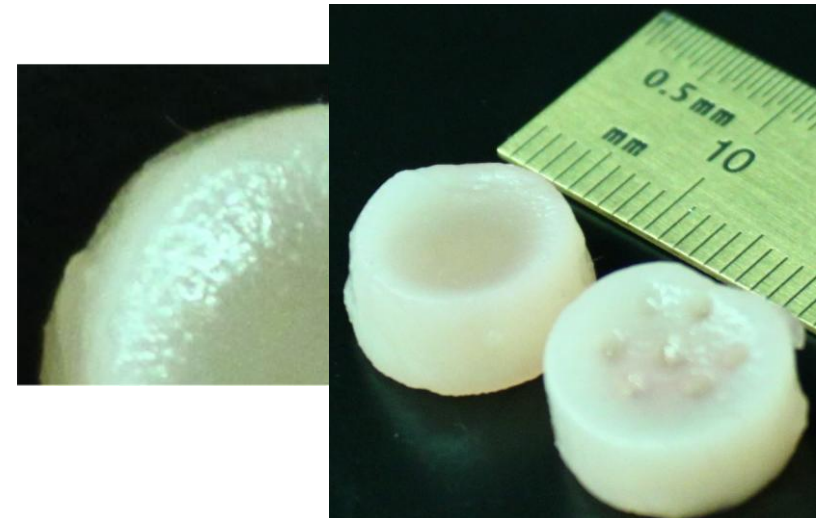
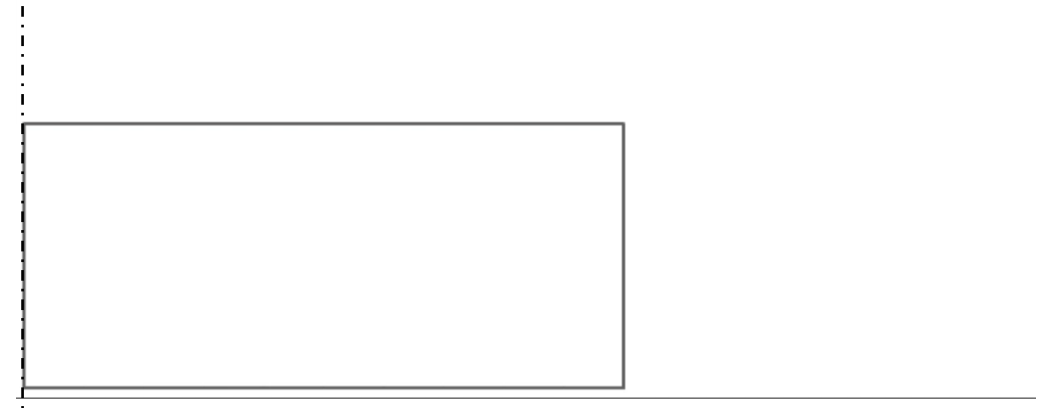


# Multiphasic Theory with Reactions

- Mixture of charged solid matrix, neutral solvent, and neutral or charged solutes (ions)
  - Triphasic theory (Lai, Hou, Mow, J. Biomech. Eng. 1991)
  - Multiphasic theory (Gu, Lai, Mow, J. Biomech. Eng. 1998)
  - Reactive mixtures (Ateshian, BMMB 2007)
- FEBio Implementations
  - Ateshian, Maas, Weiss, J. Biomech. Eng. 2013
  - Ateshian, Nims, Maas, Weiss, BMMB 2014
- Mixture momentum balance
  - $\text{div } \boldsymbol{\sigma} = \mathbf{0}$
- Mixture mass balance
  - $\text{div}(\boldsymbol{v}^s + \boldsymbol{w}) = \sum_{\alpha} \frac{\hat{c}^{\alpha}}{V^{\alpha}}$
  - $\hat{c}^{\alpha}$  =solute molar supply
  - $V^{\alpha}$  =solute molar volume
- Solute mass balance
  - $\frac{1}{J^s} \frac{D^s(J^s \varphi^f \tilde{\kappa} \tilde{c}^{\alpha})}{Dt} + \text{div } \boldsymbol{j}^{\alpha} = \varphi^f \hat{c}^{\alpha}$
- Reactions
  - $\sum_{\alpha} \nu_R^{\alpha} E^{\alpha} \rightarrow \sum_{\alpha} \nu_P^{\alpha} E^{\alpha}$
  - $\hat{c}^{\alpha} = (\nu_P^{\alpha} - \nu_R^{\alpha}) \hat{\zeta}$

# Growth

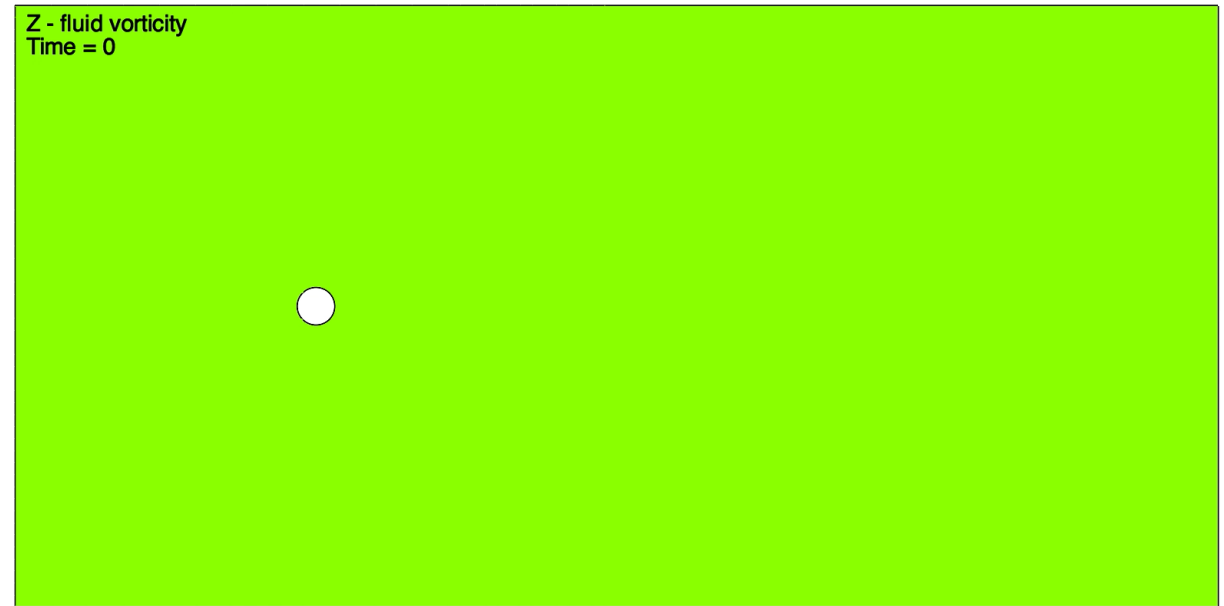
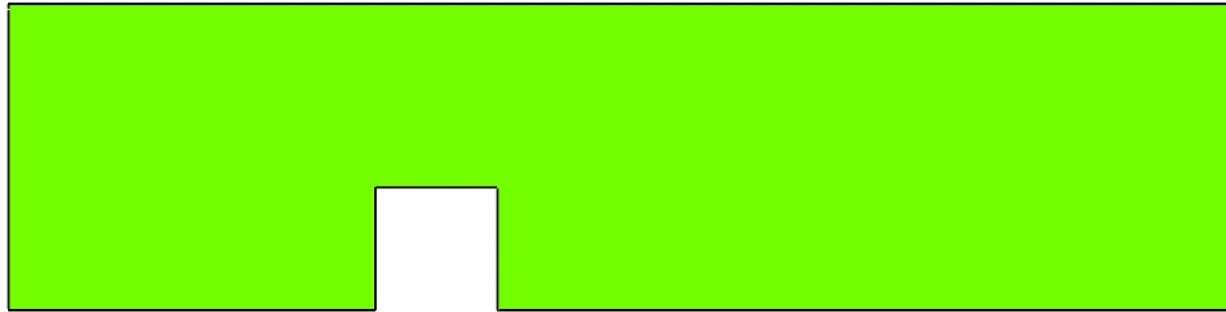
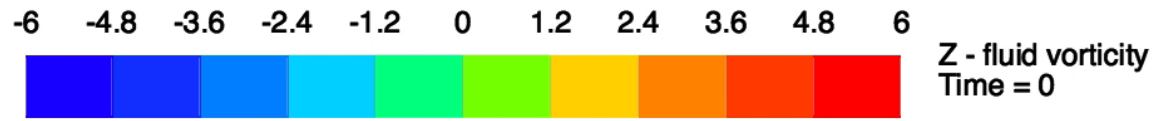
- Cartilage tissue engineering (Nims et al. 2014, 2015)
  - PG synthesis, swelling and growth
  - Mixture
    - Solid
      - agarose (neo-Hookean)
      - chondroitin sulfate ( $\text{CS}^{2-}$  as SBM)
    - Fluid
      - solvent (water)
      - $\text{Glc}$ ,  $\text{Na}^+$ ,  $\text{Cl}^-$ ,  $\text{Mg}^{2+}$ ,  $\text{SO}_4^{2-}$
    - Reactions
      - Glucose consumption by cells for homeostasis
      - $\text{CS}$  synthesis by cells consuming  $\text{Glc}$  and  $\text{SO}_4$



# Fluid Mechanics

- Solid mechanics approach (not mixture theory)
- Momentum balance
  - $\rho^f \frac{D^f \mathbf{v}^f}{Dt} = -\text{grad } p + \text{div } \boldsymbol{\tau} + \rho \mathbf{b}$
  - $\mathbf{v}^f$  =fluid velocity,  $p$  =fluid pressure,  $\boldsymbol{\tau}$  =viscous stress,  $\mathbf{b}$  =body force
- Fluid is isothermal compressible
- Mass balance
  - $\frac{\partial \rho^f}{\partial t} + \text{div}(\rho^f \mathbf{v}^f) = 0$
- Fluid volume ratio  $J^f = \det \mathbf{F}^f$ 
  - $\mathbf{F}^f$  =fluid deformation gradient
  - $\dot{\mathbf{F}}^f = \mathbf{L} \cdot \mathbf{F}^f$  where  $\mathbf{L} = \text{grad } \mathbf{v}^f$
  - Solve for  $J^f$  using  $\dot{J}^f = J^f \text{div } \mathbf{v}^f$
- Constitutive relations
  - Let  $p = p(J^f)$ , e.g.,  $p = K(J^f - 1)$  where  $K$  =fluid bulk modulus
  - Let  $\boldsymbol{\tau} = \boldsymbol{\tau}(J^f, \mathbf{L})$ 
    - Model Newtonian and non-Newtonian fluids
- FEBio implementation
  - Ateshian, Shim, Maas, Weiss, J. Biomech. Eng. 2017

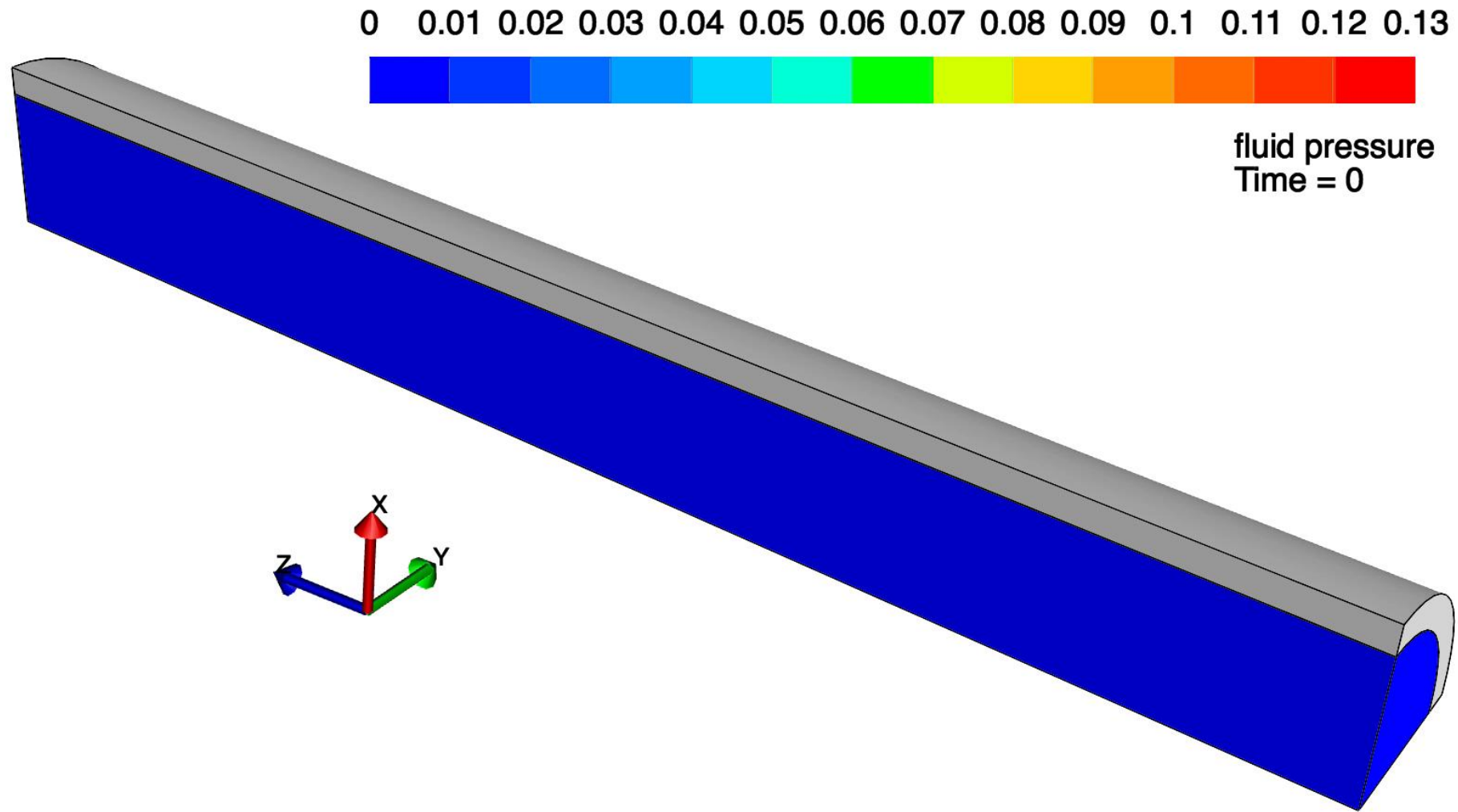
# FEBio CFD



# Fluid-Structure Interactions

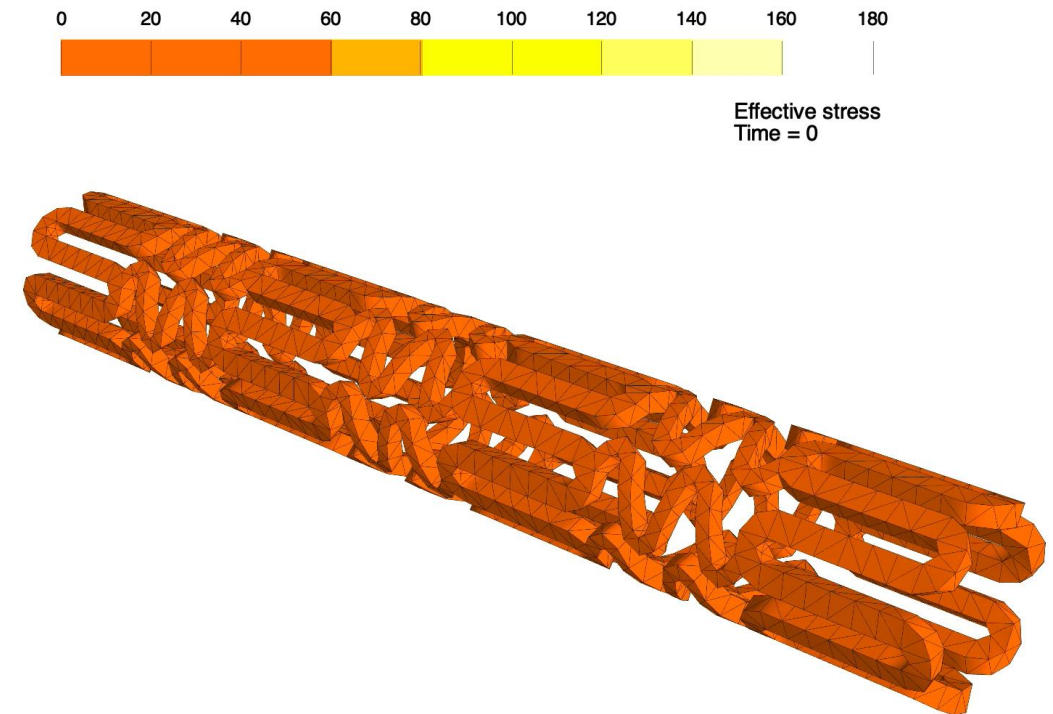
- Mixture approach
  - Fluid domain is a mixture of viscous fluid and specialized solid
  - Mesh is defined on solid. Solid has no mass and negligible stiffness
- Fluid momentum balance
  - $\rho^f \frac{D^f \mathbf{v}^f}{Dt} = -\text{grad } p + \text{div } \boldsymbol{\tau} + \rho \mathbf{b}$
- Fluid kinematic constraint
  - $\frac{D^f J^f}{Dt} = J^f \text{div } \mathbf{v}^f$
- Solid momentum balance
  - $\text{div } \boldsymbol{\sigma}^s = \mathbf{0}$
- Nodal variables
  - $\mathbf{w} = \mathbf{v}^f - \mathbf{v}^s, J^f, \mathbf{u}^s$  where  $\mathbf{v}^s = \dot{\mathbf{u}}^s$
- Use material time derivative following solid mesh
  - $\frac{D^f \mathbf{v}^f}{Dt} = \dot{\mathbf{w}} + \dot{\mathbf{v}}^s + (\mathbf{L}^f + \mathbf{L}^s) \cdot \mathbf{w}$
  - $\dot{\mathbf{w}} = \frac{\partial \mathbf{w}}{\partial t} + \mathbf{L}^f \cdot \mathbf{v}^s$
  - $\dot{\mathbf{v}}^s = \frac{\partial \mathbf{v}^s}{\partial t} + \mathbf{L}^s \cdot \mathbf{v}^s$
  - $\frac{D^f J^f}{Dt} = j^f + \text{grad } J^f \cdot \mathbf{w}$
  - $j^f = \frac{\partial J^f}{\partial t} + \text{grad } J^f \cdot \mathbf{v}^s$

# Fluid-Structure Interactions



# Additional FEBio Mixture Models

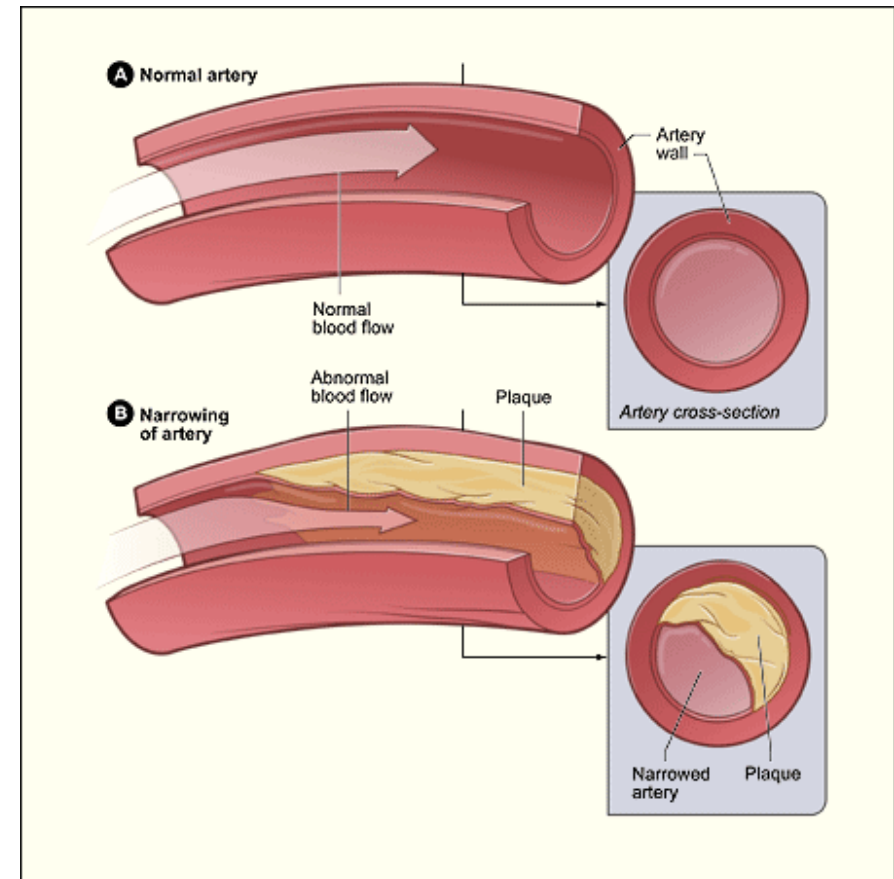
- Reactive viscoelasticity
  - Ateshian J. Biomech. 2015
- Reactive Damage
  - Nims et al. Interface Focus 2016
- Reactive Fatigue Failure
  - Zimmerman et al. WCB 2018, CMBBE 2019
- Reactive Plasticity
  - Zimmerman et al. SB3C 2019
- CFD with solutes and reactions
  - Shim et al. CMBBE 2019



Vascular stent deployment

# Pulse Wave Propagation in Stenotic Arteries

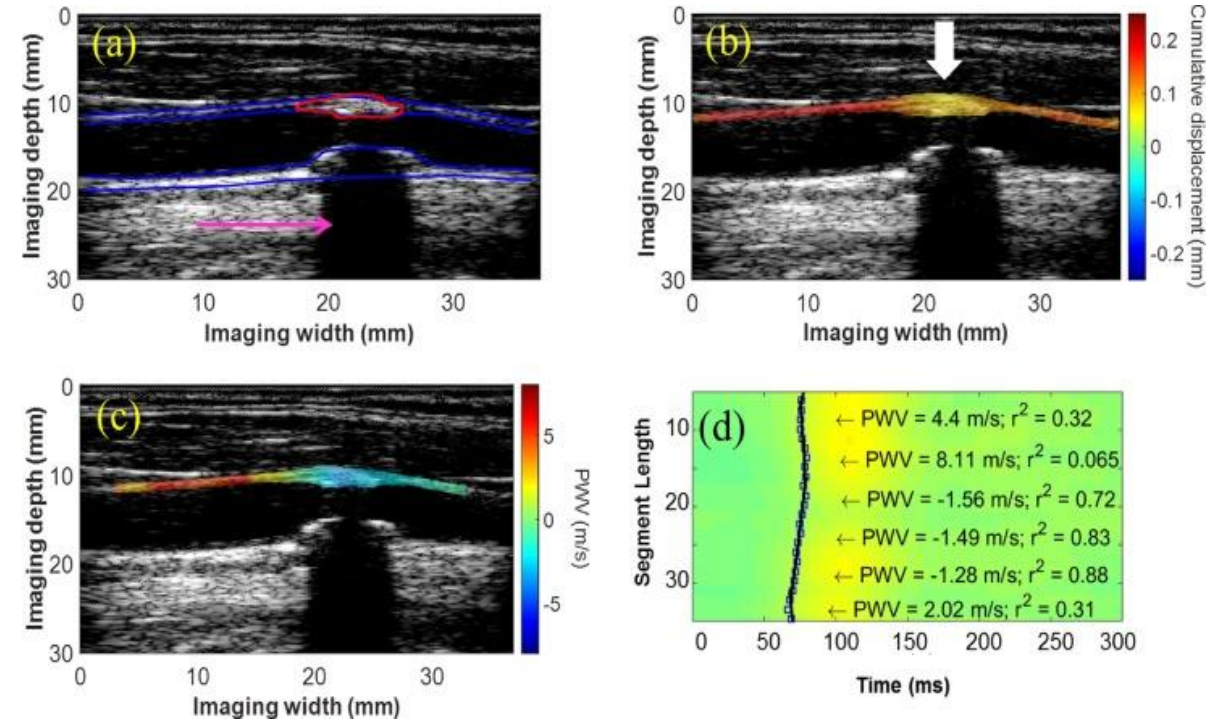
- **Atherosclerosis** is a chronic disease of the arterial wall characterized by formation of lesions and plaques
- **Rupture of vulnerable (unstable) plaques** can cause ischemic events and strokes → leading cause of death worldwide
- **Plaque characterization** is critical for diagnosis and treatment of atherosclerotic disease





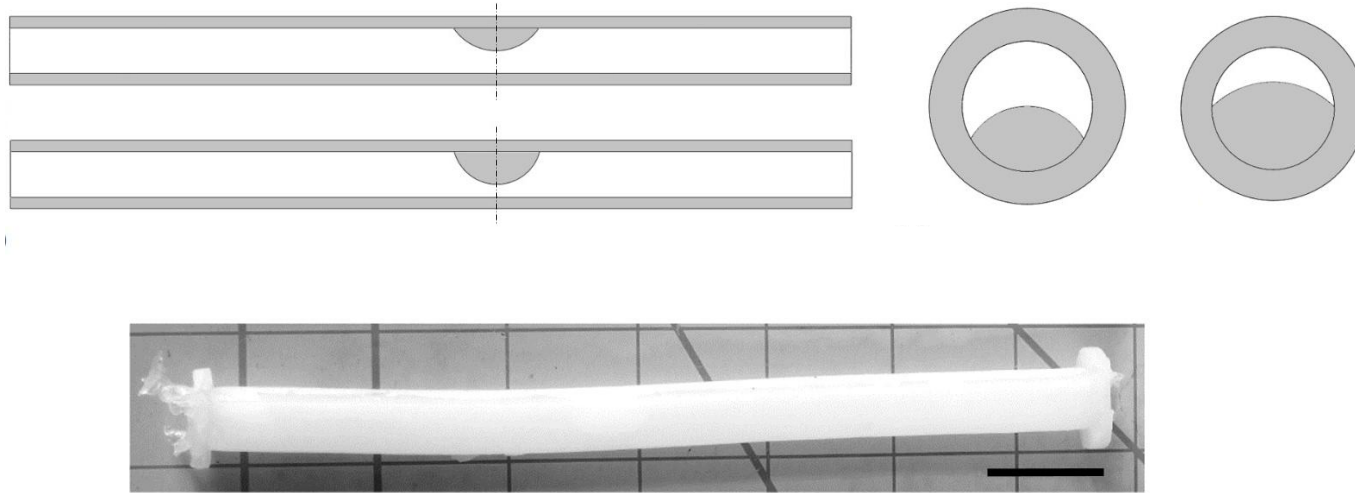
# Pulse Wave Imaging for Plaque Vulnerability

- **Pulse Wave Imaging (PWI)** is a ultrasound imaging-based technique to measure local pulse wave velocity (**PWV**) and **mechanical properties** of arterial walls
- **PWI + strain imaging** can help to differentiate plaques of varying stiffness, location and composition (**stable vs vulnerable plaques**)

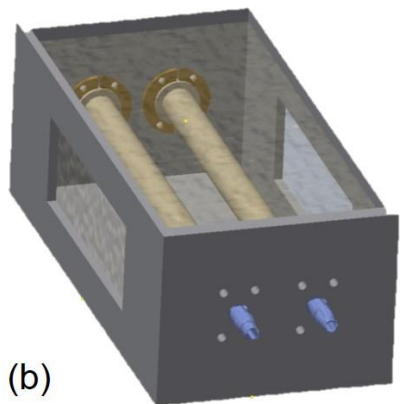


Fujikura *et al*, Ultrasonics (2007); Li *et al.*, Ultrasound Med. Biol (2019)

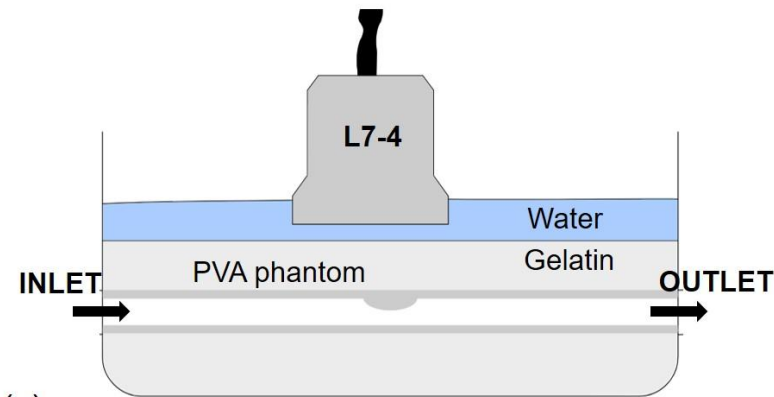
# Validation of Phantom with FE-FSI



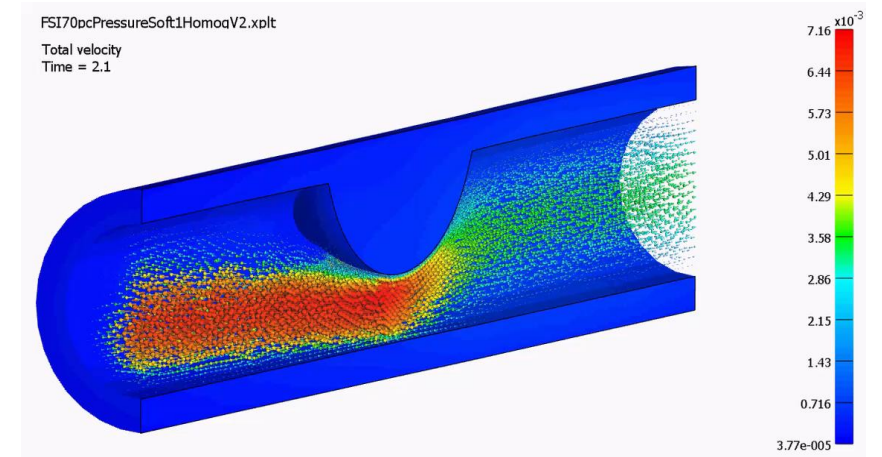
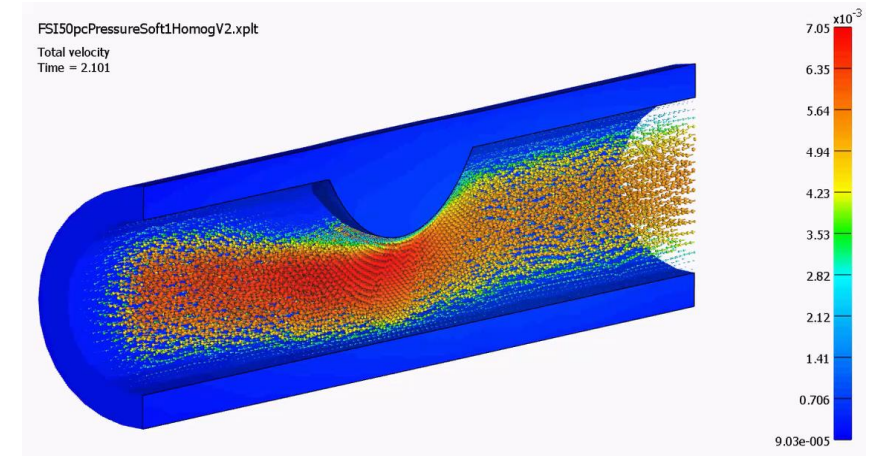
(a)






(b)

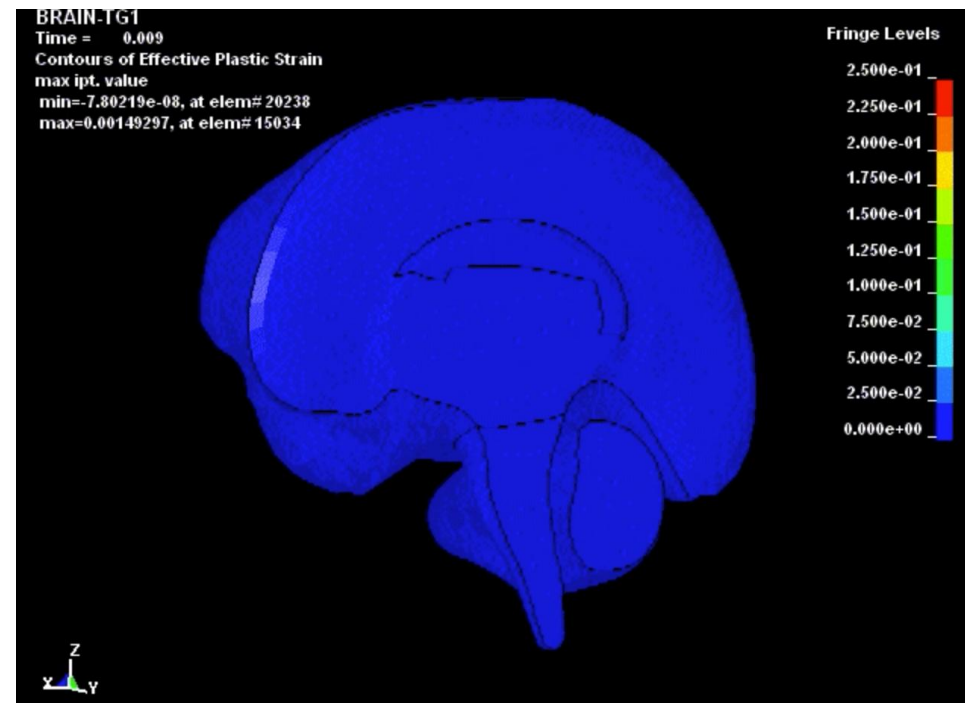


(c)



# Modeling Traumatic Brain Injury Prevention

- Mechanical Event  Biological Response
  - Initiator  Primary Injury  Secondary Injury
    - Current FE models do not simulate secondary injury

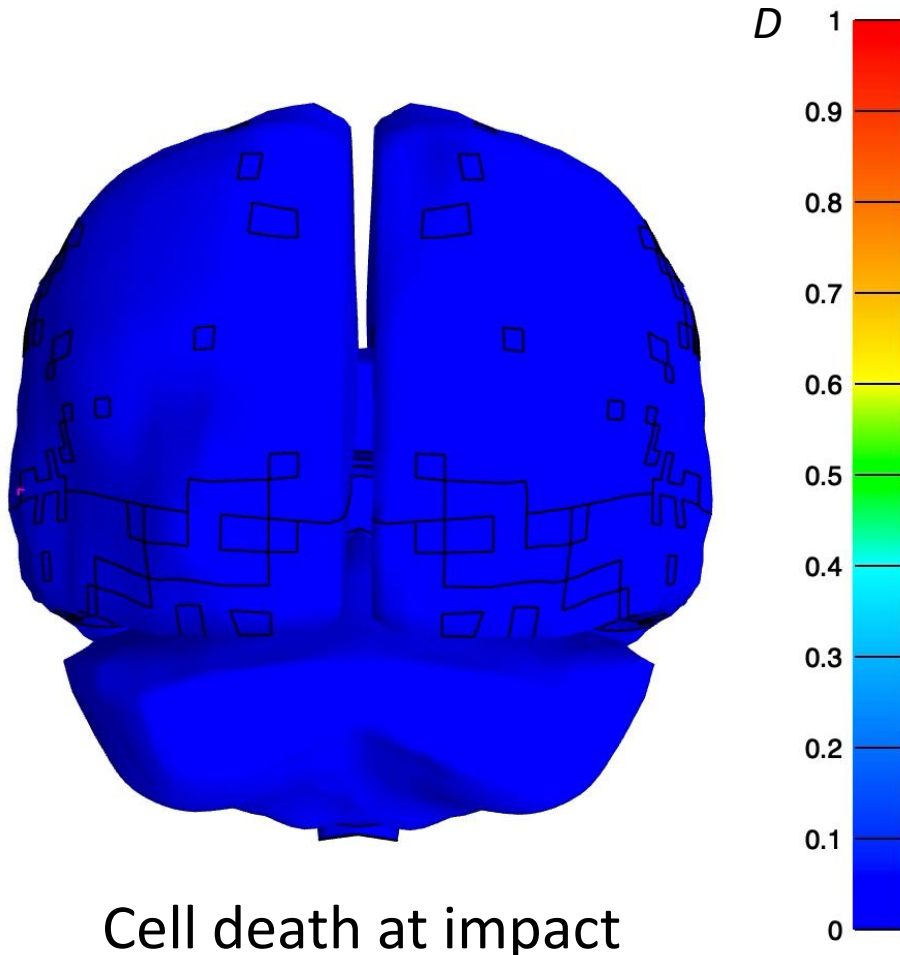


# Modeling Traumatic Brain Injury Prevention

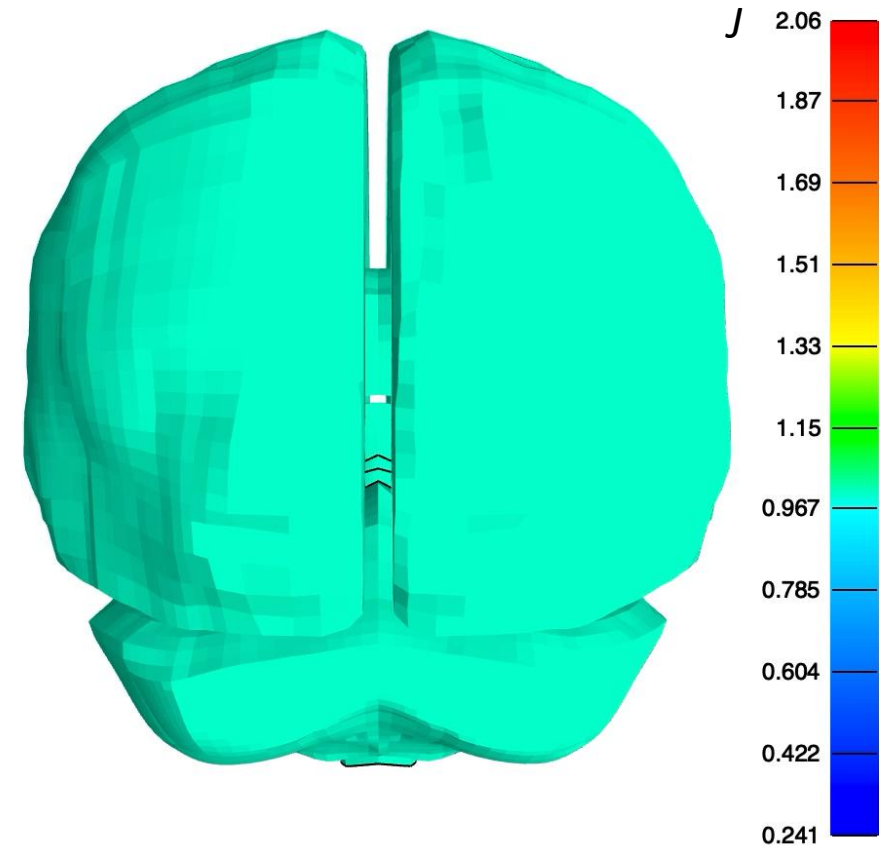
Crash Injury Research (CIREN)

database

- fatal pedestrian lateral impact
- Impact speed: 62 km/hr



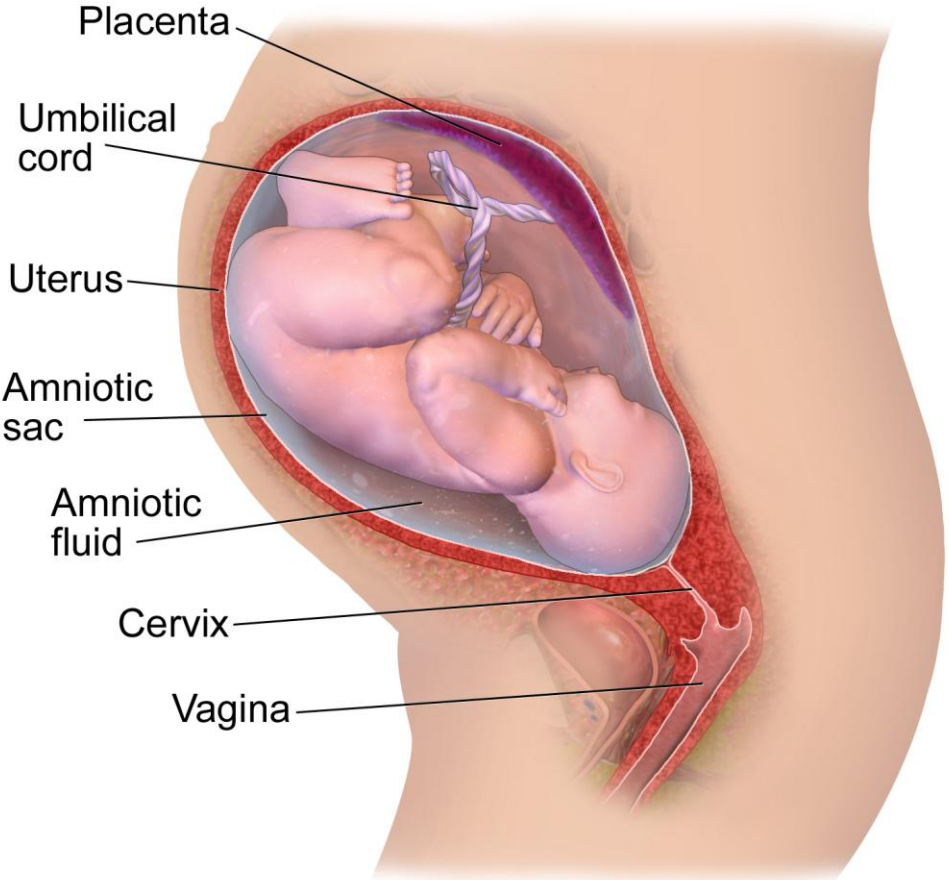
Cell death at impact



Volumetric strain

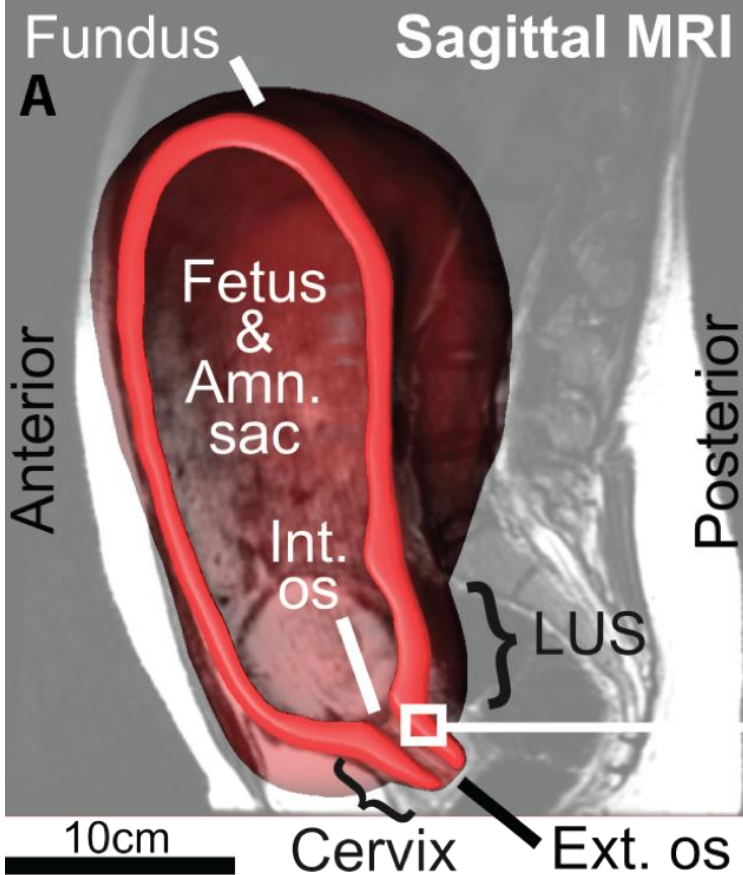
Osmotic swelling due to cell death

# Biomechanical Simulation of Pre-Term Birth

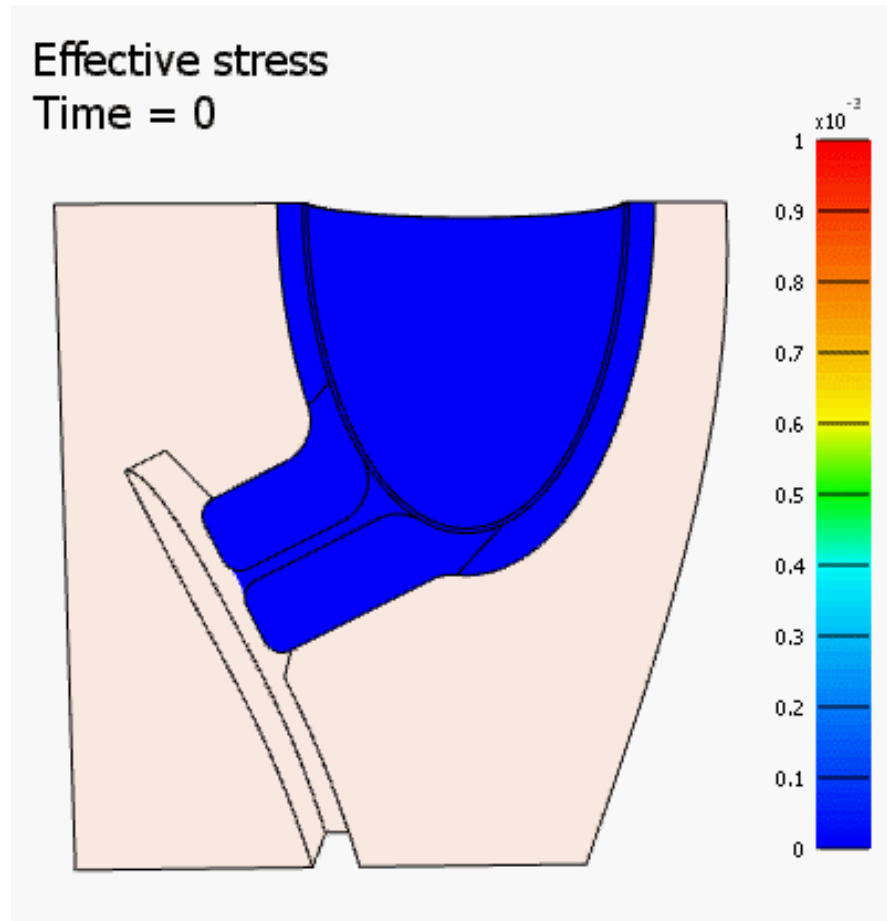


Fetal load shared by uterus, cervix, and fetal membranes

Patient-specific finite element modeling from ultrasound imaging

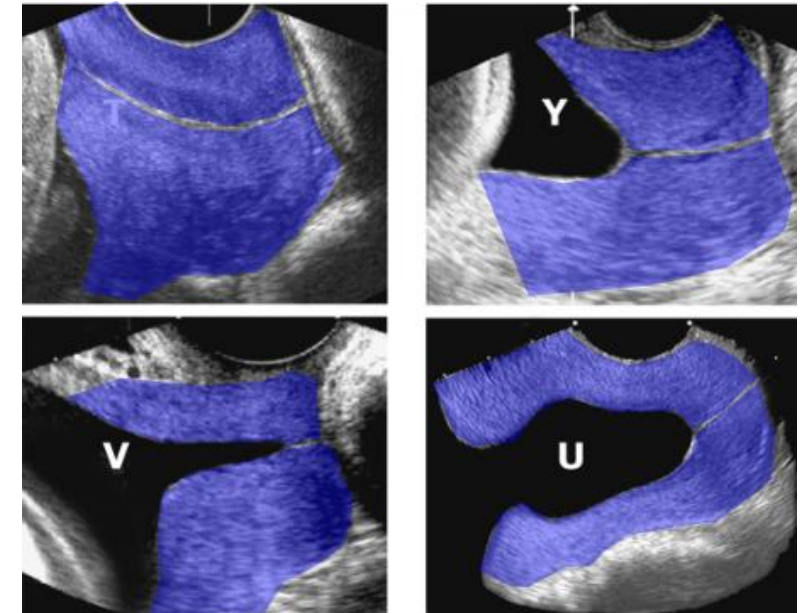


# Biomechanical Simulation of Pre-Term Birth

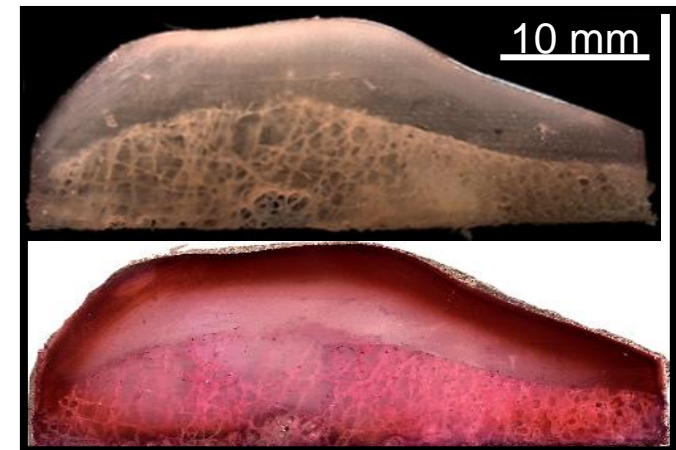
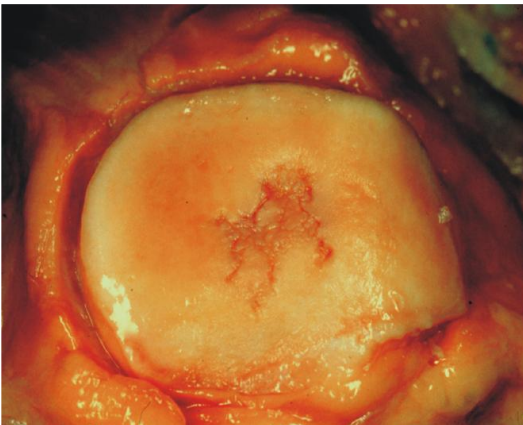
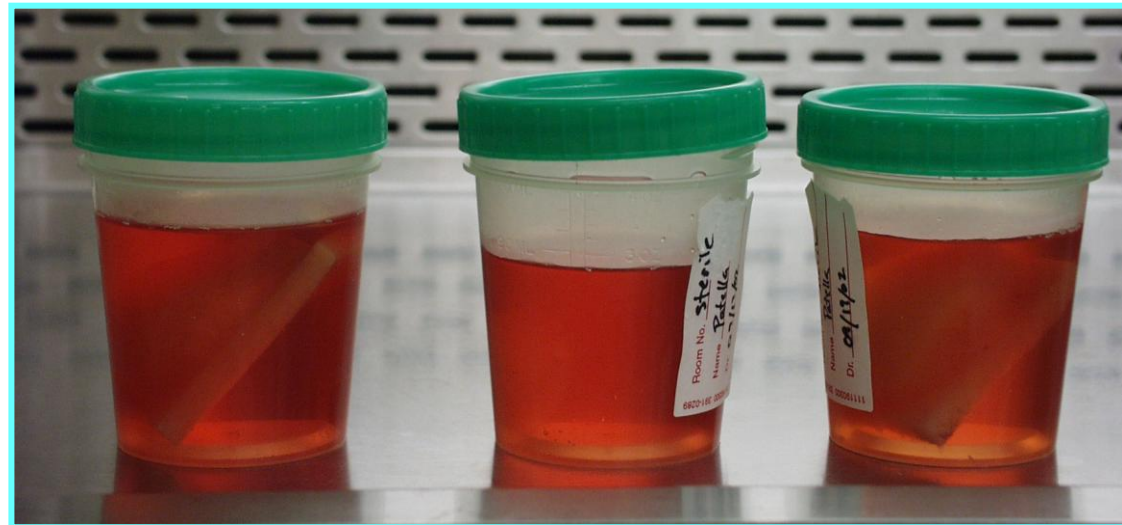
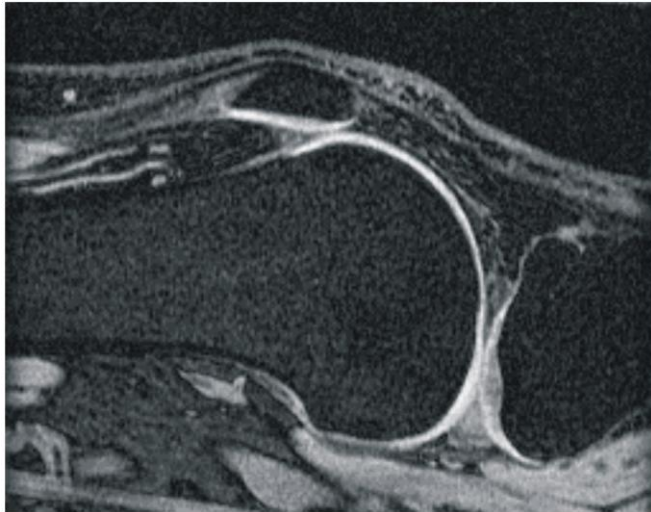


Finite element simulation of human pregnancy mid-gestation, illustrating the mechanics of clinically-observed funneling.

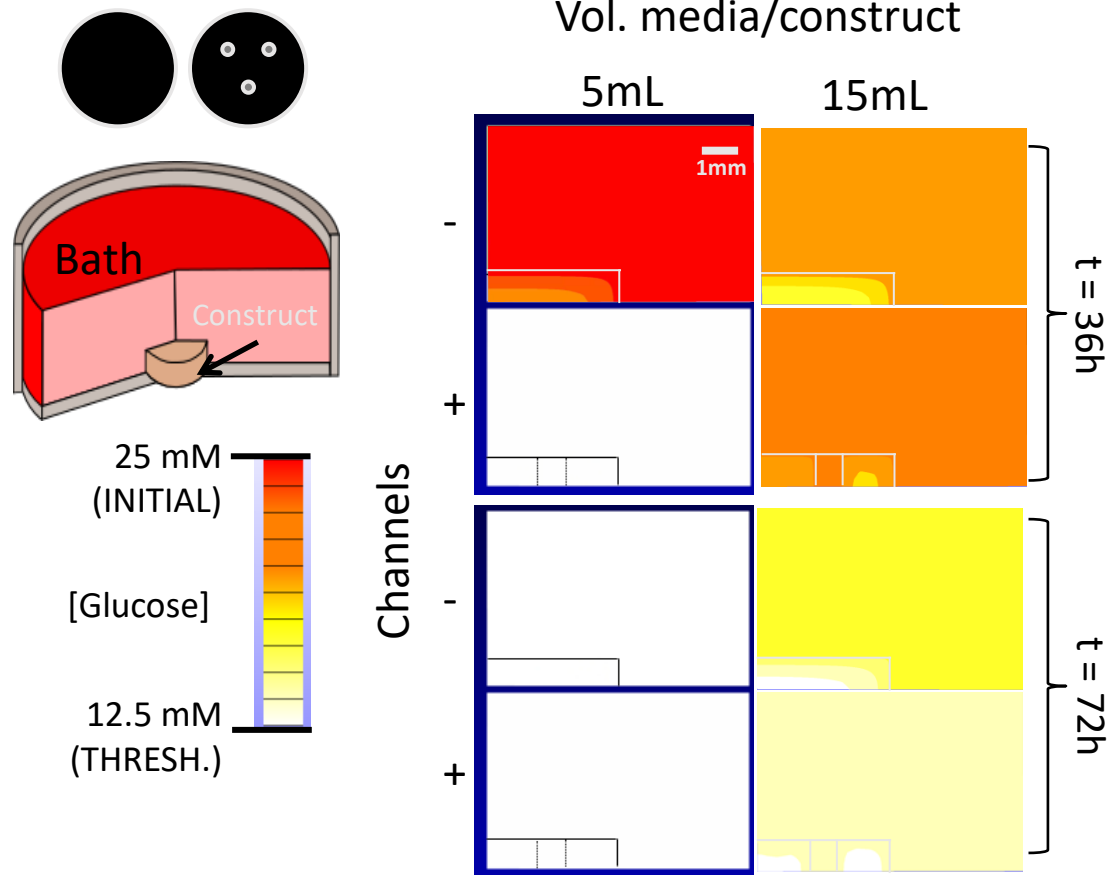
Cervical funnel shape



# Cartilage Tissue Engineering for Osteoarthritis



# Modeling Glucose Transport & Consumption





# FEBio Resources

- The place to be for
  - Executables (Windows, Mac, Linux)
  - Documentation
  - Source code

[www.febio.org](http://www.febio.org)

- Software forums:

<https://forums.febio.org>

- Plugins:

<http://febio.org/plugins/>



Github: <https://github.com/febiosoftware>



Twitter: @FEBioSoftware



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